

1 **Objectives:** The purpose of this laboratory-based study was to compare the efficacy of two
2 hearing aid fittings, with and without non-linear frequency compression, implemented within
3 commercially available hearing aids. Previous research regarding the utility of non-linear
4 frequency compression has revealed conflicting results for speech recognition, marked by high
5 individual variability. Individual differences in auditory function and cognitive abilities,
6 specifically hearing loss slope and working memory, may contribute to aided performance. The
7 first aim of the study was to determine the effect of non-linear frequency compression on aided
8 speech recognition in noise and listening effort using a dual-task test paradigm. The hypothesis,
9 based on the Ease of Language Understanding model, was that non-linear frequency
10 compression would improve speech recognition in noise and decrease listening effort. The
11 second aim of the study was to determine if listener variables of hearing loss slope, working
12 memory capacity, and age, would predict performance with non-linear frequency compression.

13 **Design:** A total of 17 adults (age: 57-85) with symmetrical sensorineural hearing loss were tested
14 in the sound field using hearing aids fit to target (NAL-NL2). Participants were recruited with a
15 range of hearing loss severities and slopes. A within-subjects, single-blinded design was used to
16 compare performance with and without non-linear frequency compression. Speech recognition in
17 noise and listening effort were measured by adapting the Revised Speech in Noise Test into a
18 dual-task paradigm. Participants were required trial-by-trial to repeat the last word of each
19 sentence presented in speech babble and then recall the sentence-ending words after every block
20 of six sentences. Half of the sentences were rich in context for the recognition of the final word
21 of each sentence and half were neutral in context. Extrinsic factors of sentence context and non-
22 linear frequency compression were manipulated, and intrinsic factors of hearing loss slope,

23 working memory capacity, and age were measured in order to determine which participant
24 factors were associated with benefit from non-linear frequency compression.

25 **Results:** On average, speech recognition in noise performance significantly improved with the
26 use of non-linear frequency compression. Individuals with steeply sloping hearing loss received
27 more recognition benefit. Recall performance also significantly improved at the group level with
28 non-linear frequency compression revealing reduced listening effort. The older participants
29 within the study cohort received less recall benefit than the younger participants. The benefits of
30 non-linear frequency compression for speech recognition and listening effort did not correlate
31 with each other, suggesting separable sources of benefit for these outcome measures.

32 **Conclusions:** Improvements of speech recognition in noise and reduced listening effort indicate
33 that adult hearing aid users can receive benefit from non-linear frequency compression in a noisy
34 environment, with the amount of benefit varying across individuals and across outcome
35 measures. Evidence supports individualized selection of non-linear frequency compression, with
36 results suggesting benefits in speech recognition for individuals with steeply sloping hearing
37 losses and in listening effort for younger individuals. Future research is indicated with a larger
38 data set on the dual-task paradigm as a potential cognitive outcome measure.

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INTRODUCTION

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Depending upon degree of high-frequency hearing loss and output limits of hearing aid receiver technology, critical high-frequency speech information is commonly not available to hearing aid users. Monson, Story, and Lotto (2014) reviewed the role of high-frequency energy (5-20 kHz) in speech and singing and discussed the importance of high-frequency energy for sound quality, localization and speech intelligibility. A number of studies have shown that difficulty perceiving high-frequency speech information can have negative consequences for speech perception (e.g., Lippmann 1996; Hogan & Turner 1998; Stelmachowicz et al. 2001; McCreery et al. 2013).

Non-linear frequency compression is a hearing aid processing strategy that is intended to restore high-frequency cues that would otherwise be unavailable to a listener with hearing loss (Simpson et al. 2005). In order to shift high-frequency spectral information from inaudible frequency regions to audible frequency regions, non-linear frequency compression algorithms use individualized compression ratios and cut-off frequencies, based upon the user's audiogram (cf., Alexander 2013). From an acoustic point of view, individuals with steeply-sloping high-frequency hearing losses, which are often observed in an older adult population, would be predicted to receive the most benefit from this processing strategy, given that previously inaccessible high-frequency cues would be compressed into an audible frequency range (Hopkins et al. 2014). Additionally, high-frequency cues have been found to be particularly helpful for speech perception when background noise is present (Baer et al. 2002; Hornsby et al. 2011). Therefore, if non-linear frequency compression successfully restores high-frequency cues, individuals who would otherwise not have access to these cues would be predicted to benefit, particularly in noisy listening conditions.

63 Alexander (2013) recently provided an extensive review of frequency-lowering
64 amplification strategies, emphasizing the individual variability in outcomes with frequency-
65 lowering strategies. Even though non-linear frequency compression is commercially available,
66 there remains conflicting evidence across numerous studies published over the last decade
67 regarding its benefit for adults using a range of outcome measures in simulations or with
68 commercial hearing aids, including consonant recognition in adults (Glista et al. 2009;
69 McDermott & Henshall 2010; Alexander et al. 2014) and speech recognition for words and
70 sentences (Simpson et al. 2005, 2006; Bohnert et al. 2010; Wolfe et al. 2010, 2011; McCreery et
71 al. 2013). Several studies have investigated the use of non-linear frequency compression with a
72 pediatric population as well, measuring its effects on phoneme discrimination, word and sentence
73 level recognition, and subjective preferences (Glista et al. 2009; Wolfe et al. 2011; Brennan et al.
74 2014). Several studies published since the Alexander (2013) review have measured speech
75 perception outcomes with non-linear frequency compression within an older adult population
76 with hearing loss using commercially-available hearing aids.

77 **Outcomes with Non-Linear Frequency Compression in Commercial Hearing Aids**

78 Ellis and Munro (2015a, 2015b) published among the few studies demonstrating benefit
79 of non-linear frequency compression for speech recognition in an adult population using
80 commercially available hearing aids. They observed significantly improved monosyllabic word
81 recognition in quiet and in noise as well as significantly improved sentence recognition in noise.
82 Recognition performance was predicted most strongly by high-frequency hearing loss.
83 However, two other recent studies demonstrated little to no benefit in a similar population using
84 different outcome measures (Hopkins et al. 2014; Picou et al. 2015). Significant improvements
85 for identification of the consonants /s/ and /t/ were found in quiet conditions, but no

86 improvement for speech recognition in noise. Aside from task differences, one possible source of
87 the variability in speech perception outcomes is the fitting algorithm used for each study to apply
88 hearing aid gain. Studies without significant improvement for speech recognition used the NAL-
89 NL1 prescription (Byrne et al. 2001), whereas studies with significant improvements in speech
90 recognition made use of the NAL-NL2 prescription (Keidser et al. 2011). NAL-NL2 provides
91 more high-frequency gain than NAL-NL1, perhaps providing greater potential benefit from non-
92 linear frequency compression. Therefore, the high-frequency gain provided by the NAL-NL2
93 prescriptive hearing aid fittings as compared to NAL-NL1 would likely result in additional high-
94 frequency cues being available after the signal is compressed.

95 Despite the variability in speech recognition outcomes with non-linear frequency
96 compression, several manufacturers automatically enable non-linear frequency compression
97 during a first-fit procedure, with the strength of the settings depending on hearing loss severity
98 and slope. When dispensing audiologists then fit to a prescriptive target following evidence-
99 based guidelines for practice (Valente et al. 2006), the clinical decision-making process then
100 turns to selecting processing features that are appropriate for the needs of the individual. It is
101 important to better understand the sources of variability in speech recognition outcomes with
102 non-linear frequency compression in order to determine which hearing aid candidates could
103 potentially benefit from non-linear frequency compression and in which listening environments
104 non-linear frequency compression may be beneficial. A better understanding of which variables
105 are driving speech perception performance with non-linear frequency compression will
106 contribute to the evidence base for patient-centered hearing aid feature selection.

107 **Cognitive Factors in Hearing Aid Outcomes**

108 An emerging area of research within the field of cognitive hearing science examines how

109 various cognitive factors in addition to hearing status influence hearing aid outcomes. The Ease
110 of Language Understanding (ELU) model proposed by Rönnberg and colleagues (2008, 2013)
111 highlights the significance of cognitive factors for the processing of speech in listening
112 conditions with varying perceptual and cognitive demands. According to this model, most
113 individuals with normal hearing sensitivity can easily process incoming speech signals rapidly
114 and implicitly (Rapid Automatic Multimodal Binding of Phonology system). Multi-sensory
115 information, namely from the auditory and visual peripheral networks, is combined within this
116 system for rapid integration of incoming sensory information. However, when the speech signal
117 is degraded either due to competing noise or hearing loss, the encoding of the speech signal may
118 not match representations within an individual's lexicon. Within the ELU model, when there is
119 mismatch between an incoming speech signal and lexical representations in memory, explicit
120 processing of the signal is assumed to become necessary to achieve speech understanding.

121 According to this model, explicit processing due to lexical mismatch is further
122 hypothesized to recruit working memory, which is the ability to maintain and manipulate
123 incoming sensory information within memory. Recruiting working memory for additional
124 processing of a distorted speech signal is hypothesized to lead to more effortful speech
125 perception. Since additional cognitive resources are allocated for the processing of the speech
126 signal, there may be fewer resources that can be allocated to provide deeper encoding of the
127 incoming message. Additionally, when context is unavailable, it is much more difficult to repair
128 the degraded signal. Some populations, including older adults, are known to rely heavily upon
129 context in order to determine the gist of a sentence or phrase (Pichora-Fuller et al. 1995; Pichora-
130 Fuller 2008).

131 Acknowledging the potential influence that cognitive factors may have on speech
132 perception, researchers have begun to measure not only the proportion of words or sentences that
133 an individual can perceive and repeat (speech recognition), but also to measure the amount of
134 listening effort that was expended for a speech perception task. Listening effort has been defined
135 as, “The mental exertion required to attend to, and understand, an auditory message,”
136 (McGarrigle et al. 2014, p. 434). Evidence from multiple studies demonstrates that older adults
137 with hearing loss expend more listening effort for perceptual processing of speech stimuli than
138 older adults with normal hearing (McCoy et al. 2005; Wingfield et al. 2005; Tun et al. 2009).
139 The additional cognitive resources expended for perceptual processing may result in a
140 “downstream effect” of fewer cognitive resources being available for further signal manipulation
141 and storage into long-term memory. One measurement method with potential for clinical
142 application in audiology is to assess listening effort using a dual-task involving memory recall of
143 speech stimuli presented for speech recognition tasks (e.g. Smith et al. 2016). If hearing aid
144 signal processing strategies help to reduce listening effort, then improvements in a secondary
145 recall task can be expected. In an examination of the benefits of hearing aid signal processing,
146 listening effort measures have been found to be sensitive to differences in the effects of signal
147 processing even when speech recognition scores remain unchanged (Sarampalis et al. 2009;
148 Hornsby 2013).

149 Sarampalis, Kalluri, Edwards, and Hafter (2009) measured listening effort with digital
150 noise reduction processing using a dual-task test method for an adult population with hearing
151 thresholds within normal limits. In the primary task, participants reported the final word of a
152 sentence presented in quiet or 4-talker babble at different signal-to-noise ratios. The secondary
153 task was to recall as many of those words as possible from blocks of eight sentences. While the

154 noise reduction algorithm under study did not improve speech recognition, it did improve recall
155 performance at the most difficult signal-to-noise ratio tested (-2 dB SNR). The benefit provided
156 by the noise reduction algorithm was hypothesized to decrease the listening effort during the
157 recognition task, possibly freeing cognitive resources within working memory for the recall task.
158 Therefore, measures of listening effort that involve a memory task in addition to a recognition
159 task may be more sensitive than measures of speech recognition alone to the benefit received by
160 hearing aid users from particular processing strategies.

161 Interpreting the findings of Sarampalis and colleagues (2009) within the ELU framework,
162 noise reduction processing may have helped to reduce the listening effort at the more difficult
163 signal-to-noise ratio by improving the acoustic content of the amplified signal, thereby
164 increasing phonological precision. The improved phonological representation of the speech
165 signal with noise reduction would mean less explicit processing would be necessary to perceive
166 the signal as compared to conditions without noise reduction. Another interpretation may be that
167 the reduction of the noise level made the noise less distracting and the signal more comfortable
168 for participants, even without direct improvements in recognition performance. Either
169 explanation would account for a reduction in the cognitive demand for the recognition task and
170 release cognitive resources for the secondary recall task.

171 Desjardins and Doherty (2014) also utilized a dual-task measure that had a primary task
172 of sentence recognition in noise with a different secondary task (visual-tracking) to assess the
173 benefits of noise reduction in a commercial hearing aid for listeners with hearing loss. They
174 found that noise reduction helped reduce listening effort in the most difficult signal-to-noise ratio
175 condition, but did not significantly improve sentence recognition in noise performance, which is
176 consistent with the findings of Sarampalis and colleagues (2009). This finding suggests that

177 although recognition performance did not significantly improve with the use of noise reduction,
178 the secondary recall task was sensitive to a reduction in listening effort.

179 In summary, studies of cognitive factors in hearing aid outcomes support the
180 measurement of listening effort in evaluations of hearing aid signal processing technology. In the
181 present study, it is hypothesized that if non-linear frequency compression can successfully
182 restore phonological cues that would otherwise be unavailable to a listener with hearing loss,
183 then it would be likely that the improved phonological encoding would reduce the listening effort
184 required, as measured using a recall task in addition to a recognition task. More specifically, the
185 partial restoration of high-frequency speech acoustic cues to individuals who would otherwise
186 not have access to them should reduce the listening effort necessary for the primary task of
187 speech recognition, releasing cognitive resources on the secondary recall task.

188 **Individual Differences in Hearing Aid Outcomes**

189 The ELU model also suggests that individuals with a higher working memory capacity
190 would be able to make better use of amplified signals provided by hearing aid processing
191 strategies (Lunner et al. 2009; Sarampalis et al. 2009; Arehart et al. 2013; Ng et al. 2013; Souza
192 et al. 2015a). Some hearing aid algorithms are intended to provide additional audibility to the
193 users, but alterations of the speech signal may also be conceptualized as a form of distortion
194 (Arehart et al., 2013; Souza et al., 2015b). Even though hearing aids do help to improve
195 audibility for a speech signal, they also alter its spectral and temporal characteristics with the use
196 of processing strategies such as noise reduction or non-linear frequency compression. Again,
197 within the ELU framework, distortion introduced by hearing aid signal processing algorithms
198 could be interpreted as inducing phonological mismatch. Individuals with higher working
199 memory capacity would then be more likely to receive benefit from the increased audibility,

200 while using their greater working memory capacity to resolve phonological mismatch. By
201 contrast, individuals with lower working memory capacity may not have the cognitive resource
202 to rapidly process the spectro-temporal alterations introduced by the signal processing strategy.
203 Previous research has suggested that working memory capacity, often measured using the
204 Reading Span Test (Daneman et al. 1980), may be a good predictor of benefit or detriment when
205 using various hearing aids programmed with noise reduction, frequency lowering, and
206 compression attack and release times (Lunner et al. 2009; Sarampalis et al. 2009; Arehart et al.
207 2013; Ng et al. 2013; Souza & Sirow 2014). Individuals with greater working memory capacity
208 have tended to receive more benefit from various hearing aid processing strategies than
209 individuals with low working memory capacity. Given that non-linear frequency compression
210 changes the spectral representations of incoming sound, working memory capacity may
211 influence recognition and recall of speech in noise while using this particular processing strategy.

212 **Current Study**

213 The purpose of the present study was to assess aided speech perception in noise and
214 listening effort with and without non-linear frequency compression, implemented within
215 commercially available hearing aids for older adults with hearing loss. A secondary goal of the
216 study was to determine how working memory, slope of hearing loss, and age (intrinsic factors,
217 c.f., Alexander 2013) contribute to individual differences in the potential benefits from non-
218 linear frequency compression. Older adults with sensorineural hearing loss were chosen as the
219 test population for this study since they commonly have high-frequency hearing loss, thus
220 potentially benefitting from non-linear frequency compression. Following from the work of
221 Sarampalis et al. (2009), a dual-task paradigm was used to measure aided benefit in recognition
222 and recall tasks for older adults with bilateral sensorineural hearing losses. Within the framework

223 of the ELU model, this test methodology should be an effective means to measure changes in
224 speech recognition and recall performance. The level of sentence context was also manipulated
225 in order to determine how context might interact with non-linear frequency compression for
226 speech perception in noise performance. It was predicted that in difficult speech recognition in
227 noise tasks, non-linear frequency compression would improve recognition performance by
228 restoring high-frequency speech acoustic cues. It was also predicted that benefit from non-linear
229 frequency compression may be more apparent when there is limited context, when listeners
230 cannot rely on top-down processing and lexical knowledge to recognize speech. Further, if non-
231 linear frequency compression improves the phonological representation of the acoustic signal,
232 thereby reducing listening effort, then performance on the memory recall task should also
233 improve.

234 MATERIALS AND METHODS

235 Participants

236 Seventeen adults with bilateral sensorineural hearing loss were recruited from the
237 University of Arizona Hearing Clinic via flyers, letters, and word-of-mouth. The average
238 participant age was 72 years (range: 57-85 years, SD: 7.6 years). All of the participants had
239 symmetrical hearing thresholds (≤ 15 dB difference between test ears at any frequency between
240 250 to 6000 Hz) no worse than 90 dB HL between 250 to 6000 Hz. Four-frequency pure tone
241 averages (0.5, 1, 2, & 4 kHz) ranged between mild to moderately-severe in degree (range: 26 to
242 69 dB HL; mean: 46 dB HL; see Fig. 1). All participants had acquired hearing loss as adults, and
243 13 participants had used hearing aids for at least one year while 4 participants did not have prior
244 experience with amplification. Audiometric slope was determined by calculating the dB/octave
245 slope of the thresholds between 1000 and 4000 Hz. Participants obtained passing scores on a

246 screening for cognitive impairment using the Mini-Mental State Examination (Folstein et al.
247 1975). All of the participants spoke American English as their primary language and were paid
248 for their participation. The Institutional Review Board at the University of Arizona approved the
249 research protocol.

250 **Stimuli**

251 The stimuli for the dual-task experiment were voice recordings of a male talker from the
252 Revised-Speech in Noise Test (R-SPIN; Bilger et al. 1984). The R-SPIN is composed of 8 lists
253 of 50 sentences with four-talker babble. Listeners were instructed to repeat the last word of each
254 sentence. Half of the sentences were high context sentences in which the final word in each
255 sentence was predictable, and half of the sentences were low context sentences in which the
256 context did not help to predict the final word in the sentence. All sentence stimuli (70 dBA) and
257 babble (variable level) were presented at 0° azimuth via a loudspeaker (NHT SuperOne, Benicia,
258 California, USA).

259 **Hearing Aids**

260 All participants wore a pair of Phonak (Stafa, Switzerland) Naida IX UP (Spice
261 Generation) hearing aids with custom foam tips for the study (Comply™ Canal Tips, Hearing
262 Components, Oakdale, MN). Individualized fitting targets were created for each participant using
263 the NAL-NL2 prescription procedure (Keidser et al. 2011). Real-ear verification measures
264 confirmed hearing aid output within ± 5 dB HL of each target frequency (250-6000 Hz) using the
265 Aurical FreeFit (GN Otometrics, Taastrup, Denmark) with an input level of 65 dBA while non-
266 linear frequency compression was turned off. The hearing aids were set to omnidirectional mode
267 with all noise management programs turned off and volume controls disabled.

268 Two hearing aid programs were created for testing: one program without non-linear
269 frequency compression and one program with non-linear frequency compression activated. The
270 non-linear frequency compression parameters were set according to the default settings
271 recommended by the manufacturer's fitting software (Phonak Target 3.0) for each participant
272 (Cutoff frequency range: 3.5-4.6 kHz; Compression ratio range: 2.3:1-2.8:1). We did not include
273 an acclimatization period; however, previous studies of non-linear frequency compression using
274 an adult population did not find any significant improvement in speech recognition performance
275 due to extended use of non-linear frequency compression (Hopkins et al. 2014; Ellis & Munro
276 2015a).

277 Audible bandwidth was calculated with and without non-linear frequency compression.
278 The audible bandwidth was defined as the total input bandwidth contained within the real-ear
279 aided output, from the lowest and up to the highest frequency at which each participant's
280 thresholds intersected with the aided output measured using real ear verification (McCreery et
281 al., 2013). The input and output bandwidth calculations were made using input-output curves that
282 were generated for each participant using an Aurical HIT test box based on stored real-ear data
283 (GN Otometrics, Taastrup, Denmark) with an input level of 65 dB SPL. Speech intelligibility
284 indices for average-level conversation at 1 meter were calculated for each participant, both with
285 and without frequency compression, using the Situational Hearing Aid Response Profile
286 (SHARP) Version 7 (Stelmachowicz et al. 2013).

287 **Procedures**

288 Participants were seated in the center of a 12' x 12' double-walled sound booth, at a
289 distance of 1 meter from a loudspeaker, which presented the stimuli from 0° azimuth at 70 dBA
290 SPL. Participants responded by repeating words aloud, and their responses were captured by a

291 ceiling-mounted microphone placed directly above the participant in the sound booth.
292 Participants were blinded to the differences in settings between the hearing aid programs.

293 Because of the potential for large variation in speech perception in noise ability between
294 participants, the signal to noise ratio (SNR) was set individually by finding the aided SNR
295 (without non-linear frequency compression) corresponding to 50% correct performance. This
296 was accomplished by varying the SNR from +20 dB to -8 dB SNR by changing the level of the
297 multitalker babble in 4 dB steps, with six sentences tested per SNR (Wilson et al. 2012). Using
298 the performance data at each SNR, the 50% correct performance point was calculated using the
299 Spearman-Kärber equation (Finney 1952). Once the 50% performance SNR was set, each
300 participant was tested with and without non-linear frequency compression in randomized order.
301 The measured 50% SNR points for our participants ranged from -2 to +7 dB SNR (Mean= 2.87
302 dB SNR, SD= 3.93).

303 The experimental tasks used modifications to the R-SPIN test procedures, similar to those
304 of Pichora-Fuller et al. (1995), which modified the test into a dual-task to measure listening
305 effort (recall) in addition to speech perception in noise performance (see also Sarampalis et al.
306 2009). On each trial, the participants heard a sentence and had the primary task of repeating the
307 last word of the sentence. After every six sentences, the participants had a secondary task of
308 recalling as many previously reported words as possible. Previous studies with this dual-task
309 method have used blocks of 2, 4, 6, or 8 sentences (Pichora-Fuller et al. 1995; Sarampalis et al.
310 2009). Pilot testing for the current study revealed that participants struggled to recall 8 sentence-
311 final words, and the sentence blocks were reduced to 6 sentences for this study. Performance was
312 scored for accuracy of recognition of the final word of each sentence and for the ability to recall
313 the sentence-final words of every 6-sentence block. Scoring procedures did not penalize for

314 recalling words out of order. Two lists from the R-SPIN were presented for each amplification
315 condition for a total of 100 sentences per condition.

316 We assessed each participant's working memory capacity using a sentence span task that
317 was a modified version of Daneman and Carpenter's (1980) Reading Span test (Waters, 1996;
318 Waters & Caplan, 2003). Participants were visually presented with a sequential list of sentences
319 to read (silently) on a computer monitor (iMo S10, Mimo Monitors, Princeton, NJ). After each
320 sentence, participants firstly made a plausibility judgment as to whether the sentence made sense
321 or not by pressing buttons on an E-prime 2.0 response box (Psychology Software Tools, Inc.,
322 Sharpsburg, PA) labeled "good" and "bad". After each block of 2 to 6 sentences, the participants
323 were tasked to recall the last word of each sentence in the order that they were presented. Test
324 scores were calculated two ways: the total number of sentence-ending words repeated aloud
325 correctly (total scoring) and the total number of words that were repeated in the proper order
326 (serial scoring).

327 RESULTS

328 Speech Recognition in Noise

329 Analysis of variance (ANOVA) was used to measure the effects of non-linear frequency
330 compression (off vs. on) and sentence context (high context vs. low context) on speech
331 recognition in noise, resulting in a 2x2 within-subjects ANOVA (Fig. 2, Panel A). There was a
332 main effect of non-linear frequency compression for the recognition of speech in noise
333 ($F(1,16)=5.72, p=0.03, \eta_p^2 = 0.26$), with higher speech recognition scores for non-linear
334 frequency compression enabled (Mean=63%, SD=12%) than disabled (Mean = 59%, SD=12%).
335 As predicted, the recognition of sentence-final words was better with high context (Mean=82%,
336 SD = 12%) than low context (Mean=36%, SD=13%), and this main effect of context was

337 statistically significant ($F(1,16)=380.48, p<0.001, \eta_p^2 = 0.96$). As seen in Figure 2, panel A, speech
338 recognition improved by a greater amount with non-linear frequency compression on compared
339 to off for low context sentences than it did for high context sentences. However, the interaction
340 between non-linear frequency compression and context was not statistically significant
341 ($F(1,16)=1.98, p=0.18, \eta_p^2 = 0.11$). At the individual level (Figure 3, Panel A), recognition scores
342 increased with the addition of non-linear frequency compression for 9 of the 17 participants,
343 ranging from 2% to 15% improvement combined across conditions.

344 **Listening Effort**

345 Figure 2, panel B illustrates performance on the recall task with and without non-linear
346 frequency compression for low and high context sentences. Recall performance was analyzed
347 using repeated measures ANOVA. The participants had significantly higher recall performance
348 ($F(1,16)=4.56, p=0.05, \eta_p^2 = .22$) with non-linear frequency compression on (Mean=57%,
349 SD=16%) than off (Mean=52%, SD=13%). There was no significant effect of context on recall
350 performance ($F(1,16)=2.09, p=0.17, \eta_p^2 = 0.12$) and no significant interaction was observed
351 between non-linear frequency compression and context ($F(1,16)=1.30, p=0.27, \eta_p^2 = 0.08$). At the
352 individual level, 11 of the 17 participants improved in recall performance (2% to 23% benefit,
353 Figure 3, Panel B). To determine whether individuals who received recall benefit from non-
354 linear frequency compression were the same individuals who received recognition benefit, a
355 simple linear regression was conducted and no significant correlation was found between
356 recognition benefit and recall benefit ($r=0.14, p=0.57$). Benefit scores were averaged across
357 context for this analysis since there was no significant interaction between context and benefit
358 from non-linear frequency compression. The lack of a significant correlation between

359 recognition and recall benefit would suggest that different individuals received benefits for
360 different reasons which are explored below.

361 **Individual Differences**

362 The second aim of the study was to evaluate the intrinsic factors that may influence
363 individual differences in aided benefit or detriment from non-linear frequency compression.
364 Based on previous studies, we examined the influence of hearing loss slope and severity, audible
365 bandwidth, working memory capacity, and age on the amount of change with non-linear
366 frequency compression for speech recognition in noise and listening effort using simple multiple
367 linear regression modeling. See Table 1 for results of correlational analysis of the predictor
368 variables. Because hearing loss slope and severity correlated significantly with one another,
369 hearing loss severity was excluded from the regression modeling. For the significant
370 improvement in recognition performance due to non-linear frequency compression, the only
371 significant predictor variable was hearing loss slope. Audible bandwidth, Sentence Span scores,
372 and age all had poor prediction values ($p > 0.20$) and were excluded from the regression model.
373 As predicted, participants with more steeply sloping hearing losses received more benefit from
374 non-linear frequency compression ($R^2 = 0.33$, $F(1,15) = 7.42$, $\beta = 0.58$, $p = 0.02$; see Fig. 4).
375 Surprisingly, Sentence Span score ($p = 0.64$) and audible bandwidth ($p = 0.23$) were not significant
376 predictors of speech recognition benefit from non-linear frequency compression and were
377 excluded from the model. Audible bandwidth was not a significant predictor even though a
378 statistically significant increase in audible bandwidth for our listeners due to non-linear
379 frequency compression was observed ($F(1,16) = 21.36$, $p < 0.001$, $\eta_p^2 = .57$) with the average
380 audible bandwidth improving from 4.3 kHz (SD=0.6) to 5 kHz (SD=1.2).

381 We used simple multiple linear regression modeling again to determine which listener
382 variables contributed most to the significant improvement in recall performance due to non-
383 linear frequency compression. The only significant predictor variable was participant age, and
384 the other predictor variables were excluded from the model. Change in recall performance
385 significantly and negatively correlated with participant age ($R^2=0.29$, $F(1,15)=6.094$, $\beta=-0.54$,
386 $p=0.03$; see Figure 5). Since age rather than working memory capacity correlated with recall
387 performance, it is possible that Sentence Span test scores alone are not enough to capture age-
388 related cognitive changes, given that the younger participants received significantly more recall
389 benefit due to non-linear frequency compression. Additionally, the correlation between Sentence
390 Span scores and age approached but did not reach significance (Serial Scoring: $r=-0.45$, $p=0.08$;
391 Total Score: $r=-0.45$, $p=0.07$). The Sentence Span mean raw scores were 43.7 items correct
392 ($SD=14.5$; Range=22-72) for serial scoring and 48.8 items correct ($SD=14.86$; Range=31-77) for
393 total scores.

394 DISCUSSION

395 The effects of non-linear frequency compression on speech recognition in noise and
396 listening effort were assessed in this study in an older adult population with hearing loss. The
397 main findings were that on average, activating the non-linear frequency compression setting
398 resulted in improved speech recognition performance for low but not high context sentences and
399 reduced listening effort. Improvements in listening to and remembering speech in background
400 babble indicate that some, though not all, adults with mild to severe hearing loss can receive
401 benefit from non-linear frequency compression in a noisy environment.

402 **Effects of Non-Linear Frequency Compression**

403 One objective for this study was to manipulate the extrinsic factor of sentence context.
404 We predicted that minimal benefit from non-linear frequency compression would be observed in
405 high context listening conditions, since participants would have access to contextual information
406 to support the explicit processing of presented sentences. Greater improvement, on average, in
407 recognition performance for low context sentences due to non-linear frequency compression was
408 observed. However, the interaction between non-linear frequency compression and sentence
409 context was not statistically significant. Conversely, the relatively good performance even
410 without non-linear frequency compression for high context sentences may have operated as a
411 ceiling effect, limiting the potential benefit from non-linear frequency compression.

412 For the sentences with high context, participants were likely able to use contextual cues
413 to predict the final word and avoid the need for explicit processing (Wingfield et al. 2015).
414 Older adults have been found to be especially proficient at making use of sentence context in
415 adverse listening conditions (e.g., Pichora-Fuller et al. 1995), which is likely why less benefit
416 from non-linear frequency compression was observed in high context than in low context
417 sentences. If true, then the use of high context sentences in Picou et al. (2015) could explain why
418 they did not observe a benefit of non-linear frequency compression for sentence recognition in
419 noise. Their study used the Connected Speech Test (Cox et al. 1987, 1988), which is rich in
420 context, allowing the older listeners to make use of their conceptual and semantic knowledge to
421 accommodate a degraded speech signal (Aydelott et al. 2010). Conversely, context neutral
422 sentences force listeners to depend more heavily on the acoustic signal (Kalikow et al. 1977;
423 Pichora-Fuller et al. 1995). In real world listening conditions, such as a conversation at a
424 restaurant with a group of several talkers, listeners with hearing loss may not always have
425 context-rich listening conditions. For example, when switching attention between multiple

426 talkers or monitoring several conversations simultaneously, the predictability of speech is
427 diminished. Listeners in noisy listening environments often do not have access to the context of
428 each conversation, especially individuals with hearing loss, and as a result they must exert more
429 effort to follow each conversation or may even avoid participation in the conversation (Pichora-
430 Fuller et al. 1995; Desjardins & Doherty 2013).

431 In the present study, we also measured aided listening effort within a dual-task paradigm
432 while using non-linear frequency compression. Previous studies using a similar paradigm found
433 reduced listening effort using digital noise reduction processing for normally hearing listeners
434 (Sarampalis et al. 2009) and adults fitted with hearing aids (Desjardins & Doherty 2014).
435 Likewise, we found recall performance on average was significantly better when non-linear
436 frequency compression was enabled. Interpreted through the ELU model, our findings suggest
437 that non-linear frequency compression may have improved the phonological representation of
438 the speech signal during the recognition task. The improved phonological representation would
439 reduce the listening effort necessary for the processing of the speech signal, enabling our
440 listeners to expend more cognitive resources on the recall task.

441 **Individual Differences**

442 A secondary goal for this study was to determine the impact of intrinsic factors of hearing
443 loss slope, working memory capacity and age on the effects of non-linear frequency compression
444 for speech recognition and recall in noise. When considering speech recognition in noise, we
445 firstly examined how individual factors related to performance while manipulating sentence
446 context. Non-linear frequency compression significantly improved recognition performance. The
447 only intrinsic factor found to correlate with non-linear frequency compression benefit for speech
448 recognition in noise was hearing loss slope; individuals who had more steeply sloping hearing

449 losses received more benefit. For demonstration purposes, Figure 6 illustrates the hearing loss
450 configuration for the participants with the least amount of recognition benefit (Group A) and the
451 most recognition benefit (Group B) from non-linear frequency compression. Note that the
452 participants who received more recognition benefit from non-linear frequency compression had
453 on average more steeply sloping hearing losses. Ellis and Munro (2015b) also found that non-
454 linear frequency compression benefit correlated with high-frequency pure tone average (2000-
455 6000 Hz). Two recent studies did not find significant improvements in speech recognition
456 performance with non-linear frequency compression possibly due to using the NAL-NL1
457 prescription gain formula, which applies less high-frequency gain than the NAL-NL2
458 prescription gain formula (Hopkins et al. 2014; Picou et al., 2015). Reduced high-frequency gain
459 would result in fewer high-frequency cues being compressed into audible frequency regions
460 potentially limiting the effect that non-linear frequency compression may have on speech
461 recognition performance. Our study, similar to the studies that did find improvements in speech
462 recognition due to non-linear frequency compression (Ellis & Munro 2015a, 2015b), made use of
463 the NAL-NL2 prescription fit formula, instead, which may have provided more high-frequency
464 cues than an NAL-NL1 prescription fitting would have.

465 We also evaluated the contribution of working memory capacity for the effect of non-
466 linear frequency compression on recall. However, in the current study, age rather than working
467 memory capacity correlated with benefit from non-linear frequency compression on recall
468 performance. Benefit of non-linear frequency compression on recall negatively correlated with
469 age, meaning younger participants received more recall benefit than older participants. Previous
470 research concerning speech perception performance with hearing aid processing strategies such
471 as digital noise reduction, frequency lowering, and compression attack and release times found

472 that potential benefit from these hearing aid strategies were positively correlated with working
473 memory capacity based on Reading Span test scores (Lunner et al. 2009; Arehart et al. 2013; Ng
474 et al. 2013; Souza & Sirow 2014), which is something we did not observe in this study. One
475 potential reason is that we made use of a different version of the measure. The original version of
476 the Reading Span test was designed to have participants recall only the last words of each
477 sentence (Daneman & Carpenter 1980), which is the method we used for this study. Other
478 studies which found the significant correlation with Reading Span test scores required
479 participants to repeat either the first words or the last words of each sentence, and the
480 participants were not informed which words were to be recalled until after each block of
481 sentences was completed. By knowing a priori that only the last words of each sentence were to
482 be recalled, it is possible that our participants were better able to make use of memory strategies,
483 such as sub-vocal rehearsal, than if they did not know which words they were going to be tasked
484 to recall. However, the participants were instructed not to rehearse the sentence-ending words
485 and the primary plausibility judgment task would have made rehearsal difficult.

486 Working memory capacity was not a significant factor in benefit from non-linear
487 frequency compression for either recall or recognition performance in our study. Others have
488 reported that the relation between working memory and response to non-linear frequency
489 compression is mixed (Ellis & Munro 2015). As discussed in a recent review by Souza, Arehart,
490 and Neher (2015a), one possibility is that within studies using commercially available hearing
491 aids, such as Ellis & Munro (2015b) and the present study, each listener received a different
492 amount of signal processing whereas in other studies showing a relationship between working
493 memory (reading span) and non-linear frequency compression, all participants received the same
494 amount of processing. It is also possible that the Sentence Span Test as a measure of working

495 memory capacity may not capture all age-related cognitive changes that may contribute to
496 speech recognition performance and potential benefit from hearing aid processing strategies.
497 Other measures that may be helpful in determining the cognitive status of participants could
498 include tests that specifically measure executive function, attention, and processing
499 speed (Akeroyd 2008). Future studies should consider the use of a broader cognitive test battery
500 to capture additional age-related changes in cognition (Rönnberg et al. 2016).

501 **Clinical Implications**

502 The present findings are relevant for clinical practice because dispensing audiologists
503 must decide when to apply non-linear frequency compression. We found improvements in word
504 recognition and recall in background babble, indicating that some, though not all, adults with
505 mild to moderately-severe hearing loss can receive benefit from non-linear frequency
506 compression in a noisy environment. These findings add to the evidence base documenting that
507 the benefit of non-linear frequency compression varies across individuals (Glista et al. 2009;
508 Picou et al. 2015). Our findings support the conclusion that non-linear frequency compression
509 may be useful for patients with steeply sloping hearing loss, though clinical expectations for the
510 amount of benefit may be tempered by an individual's age. Within our sample, the amount of
511 change in performance by enabling non-linear frequency compression in the hearing aids ranged
512 from -8% to 22% in speech recognition and -8% to 23% in scores for recall from memory.
513 Further, scores on these outcome measures were not correlated with one another, suggesting that
514 adult listeners may experience reduced listening effort even when recognition performance is
515 unchanged. Our data suggest that adults with more steeply sloping sensorineural hearing loss
516 may receive speech recognition benefit from non-linear frequency compression in low-context,
517 noisy listening conditions.

518 Taken together, these findings add to the evidence base supporting patient-centered
519 hearing aid feature selection. Specifically, the data suggest that candidacy for non-linear
520 frequency compression should be assessed on a patient-by-patient basis, taking into
521 consideration the expected variability in benefit for speech recognition and listening effort. In
522 clinical settings, assessment of hearing aid outcomes may need to go beyond measures of speech
523 recognition in noise to include listening effort (Johnson et al. 2015; Lunner et al. 2016). Future
524 research is indicated with a larger data set on the dual-task paradigm of speech recognition and
525 listening effort as a potential cognitive outcome measure that is sensitive to differences in
526 hearing technology.

527

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- 710

711 Figure Legend

712 Figure 1. The average and range of behavioral pure tone air conduction thresholds.

713 Figure 2. Boxplots for percent correct sentence-ending word recognition in noise (A) and word
714 recall (B) with non-linear frequency compression off and on. Scores were averaged across high
715 and low contexts.

716 Figure 3. Percent of sentence-ending words correctly recognized (A) and recalled (B) with and
717 without non-linear frequency compression (NFC) enabled. Participant scores are ordered from
718 least recognition benefit to most recognition benefit with non-linear frequency compression.

719 Figure 4. Correlation between the change in recognition performance with and without non-
720 linear frequency compression and slope of hearing loss, calculated as the threshold slope
721 between 1-4 kHz.

722 Figure 5. Correlation between the change in recall performance with and without non-linear
723 frequency compression and age in years.

724 Figure 6. Average pure tone thresholds for individuals who received the least benefit (-9% to
725 +5% change; Group A) and the most benefit (+5% to +22% change; Group B) for speech
726 recognition performance with non-linear frequency compression in low context sentences.

727

728

729 Table Legend

730 Table 1. Correlation table for individual predictor variables of age, four tone pure tone average
731 (PTA, 0.5, 1, 2, and 4 kHz average), slope of hearing loss (dB/octave change between 1-4 kHz),
732 audible bandwidth, and Sentence Span test total item scores. * $p < .05$, ** $p < .01$

733

734